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CLASSIFICATION OF BRAINWAVE USING DATA MINING IN PRODUCING AN EMOTIONAL MODEL

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ABSTRACT

In this paper, classification of brainwave using real world data from Parkinson's patients is presented. Emotional model is produced from the classification of brainwave. Electroencephalograph (EEG) signal is recorded on eleven Parkinson's patients. This paper aim to find the "best" classification for the emotional model in brainwave patterns for the Parkinson's disease. The work performed based on the two method phases which are using the raw data and preprocessing data. In each of the method, we performed for steps in the sum of the hertz and divided by total hertz. In the pre-processing data we are using statistic mean and standard deviation. We used WEKA Application for the classification with 11 fold validation. As a results, implecart from the classification result is 84.42% accuracy.

Keywords: Classification, Brainwave, Emotional Model, Parkinson Patients

1. INTRODUCTION

Classification of Emotional Model is the goal to find the "best" classification performed in WEKA Application. In this study, we performed for Parkinson Patients which recently, scientists realized that human brain was relevant to human emotion, and it leaded to studying of human emotion and feeling by using information from brain, including brainwave. As a result, the medical doctor using Electroencephalography (EEC) as a medical measurement technique. By the measuring the electrical potentials caused by activation of the neurons in the brain, through electrodes allocated on the scalp, information about the neurological processes in the brain, can be extracted. The author Plutchik proposed categorized emotional model, in which the eight basic emotions are defined as follows : anger, sadness, disgust, surprise, anticipation, acceptance and joy [1].

EEG can record the changes of brainwave that reflects the emotional of the patients [2, 3]. Each of the brainwave types represents the dominant of the patients. For example if in Delta it show that the situation where adults show wave sleep in babies. Moreover, EEG has high speed, non-invasive and causes no pain to the patients. As the same time, it can be recorded and analysis which can be compared to other medical imaging techniques [4, 5]. Today, it is likely that the study of the wave emitted by the brain, known as brainwave, might be the key to diagnose the health status of a status of a person and the kind of disease that a person might be suffering from, which includes Parkinson's Disease [6], Attention-Deficit/ Hyperactivity Disorder (ADHD) [7], International Affective Picture System (IAPS) [8].

The data were provided by Medical Doctor from Universiti Sains Islam Malaysia which the study focuses on the Parkinson Disease. The study is to find the "best" classification in the WEKA.

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We	are	using	the	two	methods	which	are	a)	Beta wayes are in the frequency range of 12 30

We are using the two methods which are performing raw data after medical doctor has filtering the noise and performing fase Fourier transform (FFT). Another method was performed as pre-processing were required four steps which are calculate based line, finding the range of stand deviation and convert into range in standard deviation. The conclusion of this paper, show that SimpleCart in the WEKA gave the "best" classification and consistency for all the phases for the emotional model for Parkinson Patients.

This paper is organized as follows: in the rest of this section we detail the motivation behind our paper; in section 2 we describe previous work in the area, section 3 details our proposed methodology which explain on the two work process. Followed by section 4 in which we discuss the results. Lastly, in section 5 we draw conclusions and discuss future research.

1.1 Brainwave

Brainwave, by definition, is the rapid fluctuations of voltage between parts of the cerebral cortex that are detectable with an electroencephalograph device (EEG). In the brain, there are four basic types of waves that can be distinguished. Each of these waves can be a dominant wave in a period of time.

	Tuble 1. Druth Hu	ve Clussification
Туре	Frequency (Hz) Amplitude (mV)	Normally
Delta	0.5-3 Hz, 20- 200 mV	adults <u>slow wave</u> <u>sleep</u> in babies
Theta	3-7 Hz, 5- 100mV	young children drowsiness or arousal in older children and adults
Alpha	8 - 12 Hz	closing the eyes and by relaxation
Beta	14-30 Hz, 1- 20 mV	active, busy or anxious thinking, active concentration
Gamma	30-100 Hz, 1- 20mV	certain cognitive or motor functions

Table 1 Brain Wave Classification

Each wave is identified by amplitude and in interval of frequencies [10]:

- a) Beta waves are in the frequency range of 12-30 Hz. The waves are small and fast, associated with focused concentration and best defined in a central and frontal areas. When resisting of with suppressing movement, of solving a math task, there is an increase in Beta activity.
- Alpha waves, ranging from 7.5 to 12 Hz, are slower and associated with relaxation and disengagement. Thinking of something peaceful with eyes closed should give an increase in alpha activity.
- c) Theta waves, ranging from 3.5 to 7.5 Hz, are linked to inefficiency, daydreaming, and the very lowest waves of theta represent the fine line between being awake or in a sleep state. Theta arises from emotional stress, especially frustration or disappointment.
- d) Delta waves, ranging from 0.5 to 3.5, are the slowest waves and occurs when sleeping.

1.2 Parkinson Disease

Parkinson's disease (PD) is also known as primary parkinsonism or hypokinetic rigid syndrome is a degenerative disorder of the central nervous system. The motor symptoms of Parkinson's disease result from the death of dopamine-generating cells in the substantia nigra, a region of the midbrain; the cause of this cell death is unknown [11]. Basically, what causes Parkinson's to develop in the first place is still a mystery, but scientists know that the disease process begins when the brain becomes deficient of a neurotransmitter called dopamine. With diminishing amounts of dopamine, a person with Parkinson's will develop several motor symptoms such as movement disorders, tremors, and rigidity [12].

Early in the course of the disease, the most obvious symptoms are movement-related; these include shaking, rigidity, slowness of movement and difficulty with walking and gait. Later, cognitive and behavioural problems may arise, with dementia commonly occurring in the advanced stages of the disease, whereas depression is the most common psychiatric symptom. Other symptoms include sensory, sleep and emotional problems. Parkinson's disease is more common in older people, with most cases occurring after the age of 50.[12]

In Parkinson's disease, the alterations of basal ganglia physiology may involve the alteration in the pattern of neuronal synchronisation particularly involving beta brain rhythms [13]. The level of beta synchronisation is in turn modulated by net dopamine levels at sites of cortical input to basal ganglia [14]. Dopamine deficiency as in the

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case of Parkinson's disease will disrupt the corticobasal ganglia-thalamocortical circuits, leading to pathologically exaggerated beta oscillations [15]. In short, as Parkinson's disease is a disorder that closely related to the neural and nervous system, therefore by observing the brain wave activity of a person using EEG we can diagnose if that person have possible motor symptoms of Parkinson's Disease. For instance, as explained above, a person with an exaggerated beta wave emitted by the brain most probably is suffering from Parkinson's disease.

2. PREVIOUS WORK

The research of this paper to find the "best" classification in the brainwave using WEKA. We also performed a few testing using raw data and pre-processing data. In this era, classification is widely used in pattern recognition, which includes a number of information processing problems from speech recognition and the classification of handwritten characters to fault detection in technology and medical diagnosis. WEKA is a data analysis software tool which implements a set of machine learning algorithms for data mining tasks [16].

In this study, we performed EEG into Parkinson patients, but this is not limited into medical study. There is a study on the Music Emotion Research where the goal is to quantify and explain how music influences our emotional states. They using MIDI songs in each subject with Higuchi algorithm. As for conclusion in their study familiar songs can improve accuracy of valence classification and unfamiliar songs usage can improve accuracy of arousal classification in all subjects [17]. Another study also on emotional model for music that using EEG, in which to know the mood of the patients by observing the brainwave patterns. In this study, they are using WEKA implementation which are linear regression and C.4.5 [18].

Another possible approach of brainwave classification by [19] had computed six statistical features (Mean, standard deviation, the mean of the absolute values of the first differences of the raw signals, the means of the absolute values of the first differences of the normalized signal, the means of the absolute values of the second difference of the raw signals, the means of the absolute values of the second differences of the second differences of the normalized signals) from EEG data and the highest classification rate at 95%. In author [20], had also studied on classifying emotions from EEG signals brainwave using two

simple patter classification methods K Nearest neighbor (KNN) and Linear Discriminant Analysis (LDA) for classifying emotions.

In this study, we performed the comparison between raw data and pre-processing data. In the pre-processing data we used statistical data. We are using real world data from Parkinson patients. Enter the text here

3. METHODOLOGY AND DATA SETS

In this section will explain the work process, method and data sets. In the method will show how the calculation based line, finding the range of standard deviation, converts into range in standard deviation.

3.1 Work Process

In this paper highlighted, the two phases of work process. The first phases have four type of testing which are the raw data, the sum of the hertz based on Delta, Theta, Alpha and Beta as shown in table 1. The third types are the sum of the hertz and divided the total of hertz and lastly the sum of the hertz and divided the sum of the hertz. The second phases of work process, we performing statistical method in calculating baseline, standard deviation and mean as per-processing. Then we performed same as the first phases which has four types of testing. Then use WEKA to find the "best" classification. This is only a preliminary study to find the "best" classification for Emotional Model for Parkinson.



Fig 1: First Phase Work Process In Classification Of Brainwave

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Fig 2: Second Phase Work Process In Classification Of Brainwave

3.1 Method

In the following sections we present the methods that we have used in this paper.

Step 1:- Data gathering

The data from Parkinson collected from Faculty of Medicine, USIM. The brainwave was collected from the frontier of the head.

Step 2:- Design Model for raw data.

The emotional model will be tested for finding the relevant in using the four types of testing.

Step 3:- Pre-processing

The collection of data will be removed with all unclean data which we performed manually show in the Fig 2.

Step 4:- Design Model for Pre-Processing The emotion model will be tested for finding the relevant, intelligent classifier using pre-processing data.

Step 5:- Classification

The emotion model will be classified based on table 1 using WEKA Application. We did not use Gamma because the data only on cognitive and motor function which is not reliable for Parkinson patients.

3.2.1 Pre-processing

In the pre-processing, we performed two methods which are statistical method and classification.

3.3.2 Statistical method

In the statistical method we used three steps which are finding baseline, standard deviation and ensure the range in the standard deviation. As for the finding baseline, the medical doctor will determine the baseline. All the data will convert into baseline in Eq (1). The lacking of the process, the baseline cannot be counted and lose of information. The main (ρ) will be found in new data (T) based on the second in Eq(2). The standard deviation (σ) is to ensure the new data (T) are in the range based on the Eq(4). If the new data (T) are not in the range of the Eq(4) then the new data(T) will be changed in to (σ).

x - raw data

- *j* baseline (choose by medical doctor)
- T new data after converted into baseline
- ρ Mean of the data after converted into baseline

$$T = \left(\frac{x-j}{j}\right) \times 100 \tag{1}$$

$$\rho = \frac{1}{N} \sum_{i=1}^{N} \mathbf{T}_{i}$$
(2)

$$\sigma = \sqrt{\frac{1}{N} \sum_{i=1}^{N} \mathbf{T}_{i} - \mathbf{\overline{T}}}$$
(3)

 $p - (\sigma * 1.5) \le T \ge \rho + (\sigma * 1.5)$ (4)

$$T = \begin{cases} 1, \text{if } T = \sigma \\ T, \text{Otherwise} \end{cases}$$
(5)

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3.3.3 Classification

4. **RESULTS**

In the classification, we performed preprocessing which consists of four phases in finding the "best" classification in WEKA. This is only a preliminary study. In the future, the classification will be developed in Matlab. In the testing part we classification raw data (x) and new data (T) after pre-processing. The second testing, we perform the sum of the Hertz, the third part the sum and divided by the number of Hertz and last part by summing all the hertz and divided by the total Hertz.

3.3.4 Attribute

In the attribute we used as shown in the table 2 that used in WEKA. The brain attribute is changed for of the sum of the Hertz, sum and divided by the number of Hertz and sum all the hertz and divided by the total hertz.

Attributes	Description
Patient	Information about Patient
Class	Based on the second capture
	which are 5 second =1, 10 second
	= 2, 15 second $= 3$ and 20 second
	= 4
Domain	The domain based on the delta,
	theta, alpha and beta
Location	Location of the brainwave cap
	which are F3, Fz, F4, C3, Cz,
	C4, P3, Pz, P4.
Brain	Result capture from the
	brainwave

Table 2. Attribute Classification

3.4 Data Set

EEG data were recorded from eleven Parkinson's patients after undergoing non-invasive magnetic stimulation, a form of therapy to alleviate the motor symptoms of Parkinson's. in order to look at the acute effects of the stimulation, we analyzed the EEG data recorded 20 seconds poststimulation. The data set were taken from the medical faculty of Universiti Sains Islam Malaysia (USIM), Pandan Indah, Kuala Lumpur. The raw data has been converted into Fast Fourier Transform (FFT) using Brainwave software. This section shows all the results for classification with 11 fold cross validation and the choosing domain in hertz in WEKA.

4.1 Method 1

In this experiment, we performed the raw data and sum of the frequency (hertz). In the table 3 show the result of raw data and table 4 shows all the results on the sum of the hertz performed all the classifier in the WEKA. Table 5, result in WEKA for the sum of the hertz and divided into number of hertz. And lastly table 6, result in using WEKA for sum of the hertz and divided into total of hertz.

From the result, it show that result overall from Table 3 until Table 6 the "best" result from the SimpleCart method under classification tree. The data from raw data produced the highest result among others with 80.84% percentage of correct and follow by sum of herts and divided into total of hertz which is 76.83%. Then sum of the hertz and divided into number of hertz which is 72.54 and lastly sum of the hertz which is 57.50%.

Fig1 and Fig2 show the information output from the SimpleCart information. From the Fig1, it show that we have 11880 data with 5 attributes show in the Table 1 and using 11 fold cross validation. From the Fig2 show that the tree is interpreted using the If-Then rules:

If (Hertz < 1.4741) If (hertz < 0.3835 If (location = F3 or Fz or F4) If (hertz < 0.14565 If (hertz < 0.10456) then Beta If (hertz >= 0.10455) Location = Fz Patient < 351 If class = (20 second or 15 second or 10 second) then Beta else Checking other patients

From the analysis and trace output from the SimpleCart it the algorithms classify the hertz then the location and lastly the class and patients. It show that of the hertz between 1.4741 and 0.1055, has been classify in Beta for the patient 351. It gave the highest result in classify based on the hertz and using tree methods.

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Table 3. Result In Using WEKA For Raw Data

	Percen				
Method	tage	Percentage			
	Correct	Incorrect (%)			
	(%)				
Cla	assification l	Bayes			
NaiveBayes	71.85	28.14			
Class	sification Fu	nctions			
MultilayerPer	75.13	24.86			
ceptron					
Classification Lazy					
IBK	75.90	24.09			
Cl	assification	Meta			
Classification	80.78	19.21			
WithRegression					
Cl	assification	Misc			
VF1	61.85	38.14			
Cla	Classification Rules				
DecisionTabl	78.76	21.23			
e					
Classification Tree					
SimpleCart	80.84	19.15			

Method	Percentage Correct (%)	Percentage Incorrect (%)			
Classification Bayes					
BayesNet	58.14	41.85			
Classification Functions					
Multilaye	61.17	38.82			
r Perceptron					
Classification Lazy					
Kstar	60.60	39.39			
Classification Meta					
	Т	1			

 Table 5. Result In Using WEKA For Sum Of The Hertz

 And Divided Into Number Of Hertz.

Classification Meta				
Classifica	69.69	30.30		
tionViaRegr				
ession				
Classification Misc				
VF1	48.10	51.89		
Classification Rules				
Ridor	64.64	35.35		
Classification Tree				
SimpleCa	72.41	27.58		
rt				

Table 4. Result In Using WEKA For Sum Of The Hertz

Method	Percentage Correct (%)	Percentag e Incorrect (%)			
(Classification Bay	/es			
NaiveBayes	44.31	55.68			
Cla	ssification Func	tions			
SimpleLogi	46.02	53.97			
stic					
Classification Lazy					
Kstar	43.37	56.62			
(Classification Meta				
RotationFor	56.18	43.81			
rest					
	Classification Mi	sc			
VF1	43.24	56.75			
Classification Rules					
Decision	51.19	48.89			
Table					
Classification Tree					
SimpleCart	57.70	42.29			

 Table 6. Result In Using WEKA For Sum Of The Hertz

 And Divided Into Total Of Hertz

Method	Percentage Correct (%)	Percentage Incorrect (%)			
	Classification Ba	yes			
Naivebayes	63.57	36.42			
Simple					
Cl	assification Func	tions			
Logistics	72.22	27.77			
Classification Lazy					
Kstar	69.63	30.36			
	Classification M	eta			
Classificati	79.29	20.70			
onViaRegress					
ion					
Classification Misc					
VF1	59.94	43.05			
Classification Rules					
Ridor	70.77	29.22			
Classification Tree					
SimpleCart	76.83	23.16			

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=== Kun inior	Hellon ===		
Scheme:weka.c	lassifiers.trees.SimpleCart -S 1 -M 2.0 -W 5 -C 1.0		
Relation:	1. Data_BeforeProcess_Format1-weka.filters.unsupervised.attribute.Discretize-B10-M-1.0-Rfirst-last		
Instances:	11880		
Attributes:	5		
	Patient		
	Class		
	Domain		
	Location		
	Dumeric		
Test mode:11-	fold cross-validation		

Classification Lazy				
Kstar	61.21	38.78		
Classifi	cation Met	a		
RotationForrest	62.91	37.08		
Classifi	Classification Misc			
VF1	20.12	79.87		
Classification Rules				
Jrip	62.79	37.74		
Classification Tree				
SimpleCart	62.79	37.20		

Table 8. Result In Using WEKA For Sum Of The Hertz For Pre-Processing Data

Method	Percentag e Correct (%)	Percentag e Incorrect (%)		
C	assification Bay	es		
NaiveBayes	31.48	68.51		
Clas	sification Funct	ions		
Multilayer	37.37	62.62		
Perceptron				
С	lassification Laz	y		
Kstar	33.16	66.62		
Classification Meta				
Stacking	25	75		
С	Classification Misc			
Hyperpipes	33.92	66.07		
C	Classification Rules			
OneR	39.81	60.18		
Classification Tree				
RepTree	35.01	64.98		

Table 9. Result In Using WEKA For Sum Of The Hertz And Divided Into Number Of Hertz For Pre-Processing Data.

Method	Percentag e Correct (%)	Percentag e Incorrect (%)	
С	lassification Bay	/es	
BayesNet	32.15	67.84	
Clas	ssification Funct	tions	
RBFNetwor	33.50	66.49	
ks			
Classification Lazy			
Kstar	27.86	72.13	
Classification Meta			
Classificatio	45.20	54.79	
nViaRegressio			

Fig1: Information Output

CADT	Decision	7200
CHKI	Decision	Ttee

- Numeric < 1.4741
- | Numeric < 0.3835
- | | Numeric < 0.14675: Beta(2557.0/66.0)
- | | Numeric ≻= 0.14675
- | | Location =(C3) | (C4) | (Cz) | (F3) | (F4) | (Fz)
- | | | Location =(C3)|(C4)|(Cz)|(F3)|(F4)|(P3)|(P4)|(Pz)
- | | | | Location = (C3) | (C4) | (Cz) | (Fz) | (P3) | (P4) | (Pz)

Fig 2: Information Output

4.2Method 2

In this experiment, we performed statistical method such as finding baseline, standard deviation and ensure the range in the standard deviation. As for the finding baseline, the medical doctor will determine the baseline. The baseline will not be used in the pre-processing using WEKA. From the experiment, it show that SimpleCart is the "best" classification in WEKA in all the types testing expect in sum of the hertz which is stacking.

Table 7. Result In	Using	WEKA	For Pr	e-Processing
Data				

Method	Perce ntage Correct (%)	Percentag e Incorrect (%)	
Classification Bayes			
BayesNet	62.40	37.57	
Classification Functions			
MultilayerPerceptro	62.75	37.25	
n			

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n				
0	Classification Misc			
Hyperpipes	25	75		
Classification Rules				
Ridor	39.56	60.43		
Classification Tree				
SimpleCart	47.39	52.60		

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produce the "best" result in the classification but not in the confusion matrix which the sensitivity are less than 80% except Beta. In the specificity are more than 100%. The next stages will target the sensitivity in Delta, Theta, Alpha and Beta more than 90%.

Table 11. Confusion Matrix

	Pre	diction
	True	True
	Positive (TP)	Negative
Actual		(TN)
Actual	False	False
	Positive (FP)	Negative
		(FN)

Table 10.	Result In Using	g WEKA For	Sum Of The Hertz	
And Divid	ed Into Total H	Iertz For Pre	e-Processing Data.	

	Perc	Perce	
Method	entage	ntage	
	Corre	Incorrec	
	ct (%)	t (%)	
Classification	n Bayes		
BayesNet	55.55	44.44	
Classification 1	Functions		
MultilayerPerceptron	59	41	
Classificatio	n Lazy		
Kstar	54.7	45.20	
	9		
Classificatio	n Meta		
ClassificationViaRegress	61.9	38.04	
ion	5		
Classification Misc			
VF1	43.6	56.39	
	0		
Classificatio	n Rules		
Ridor	57.4	42.59	
	0		
Classificatio	n Tree		
SimpleCart	64.3	35.60	
-	9		

4.3 Confusion matrix

The confusion matrix that helps detailed analysis than accuracy. Accuracy is not a reliable metric for the real performance of a classifier, because it will yield misleading results if the data set is unbalanced (that is, when the number of samples in different classes vary greatly). The utilized confusion matrix consists of TP (True Positive), TN (True Negative), FP (False Positive) and FN (False Negative) values, as shown in Table 11. Sensitivity is the calculation of the actual correctly identified instances, while Specificity the calculation of correctly identified negatives. Eq 6 and Eq 7 show the calculation on the sensitivity and specificity. The result of the confusion matrix show in Table 12 which highlighted that SimpleCart in Classification Tree

sitivity -	Number of true positi	(6

```
Number of true positive + Number )
```

 $Specificity = \frac{\text{Number of true negat}}{\text{Number of true negative} + \text{Number}} (7)$

Table 12.	Confusion	Matrix	For	Simpleca	ırt.
-----------	-----------	--------	-----	----------	------

	Delta	Theta	Alpha	Beta
Specificity	97.76	94.06	93.73	91
Sensitivity	76.01	66.10	55.66	97.20
Precision	79.00	63.11	64	94.18
Accuracy	95.58	90.33	87.39	94.71

5. CONCLUSION

In conclusion, we have performed a real data from the Parkinson patients with two methods which are real data and pre-processing data. The result shows that SimpleCart from the decision tree gave the "best" classification results in WEKA. In the SimpleCart method, they perform the If-Then statement. In future,

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we will further our study to find the emotional of the Parkinson patient and develop into Matlab software.	Frequency Bursting." Front Neural Circuits, 3.20. [11]Feinson. M., Kreinin. B., Chistyakov. A., &				
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